‘Modern’ dose distributions: what should we not forget?

Uulke van der Heide

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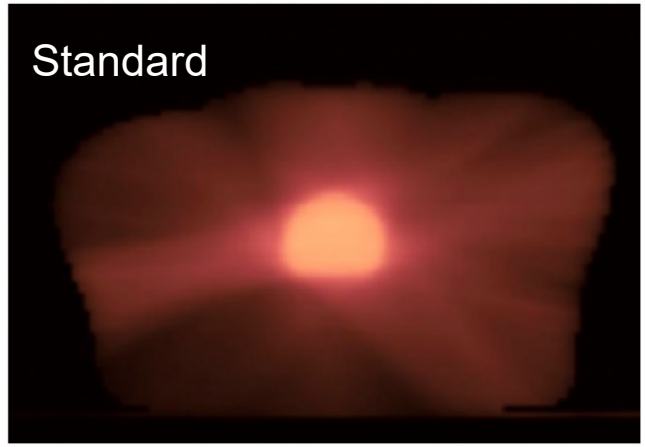
Using CT to delineate the target volume

Example: prostate cancer

Standard: homogeneous dose to entire prostate

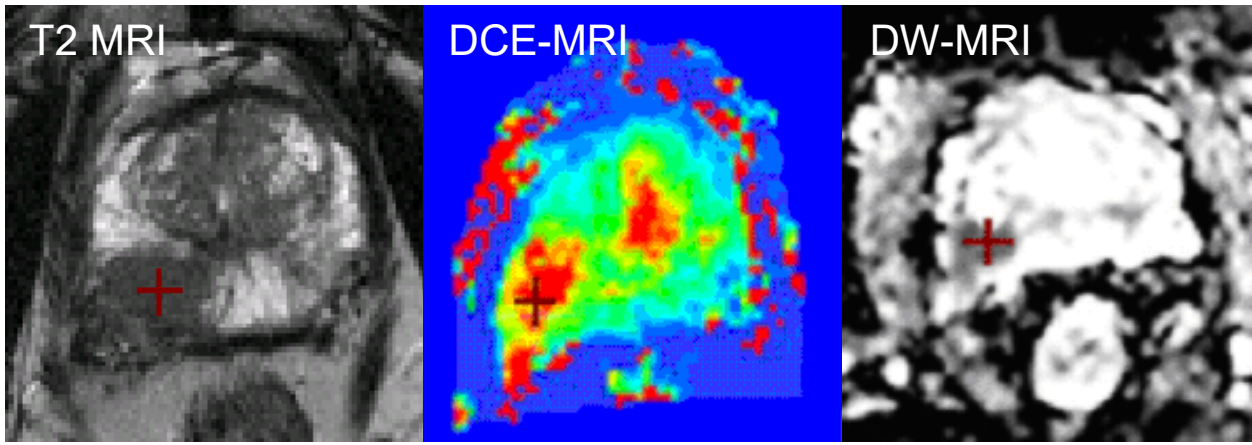


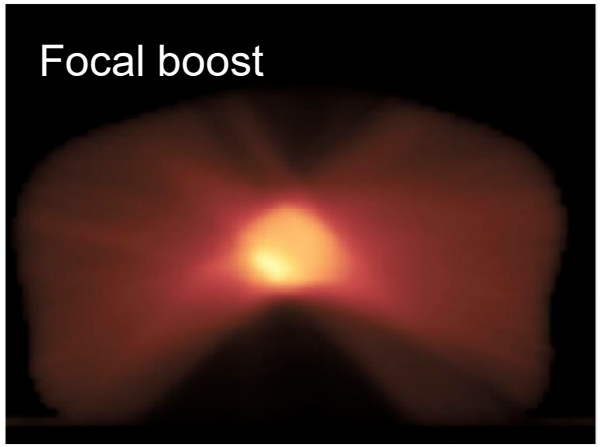
Using multi-parametric imaging to differentiate dose inside the target volume

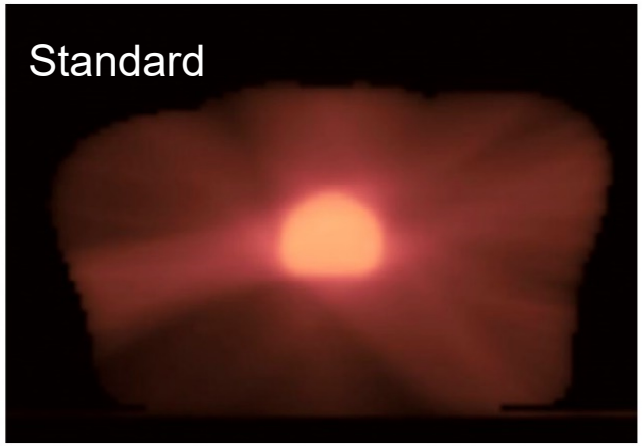
Example: prostate cancer

Standard: homogeneous dose to entire prostate

New: escalate dose at location of highest tumor burden







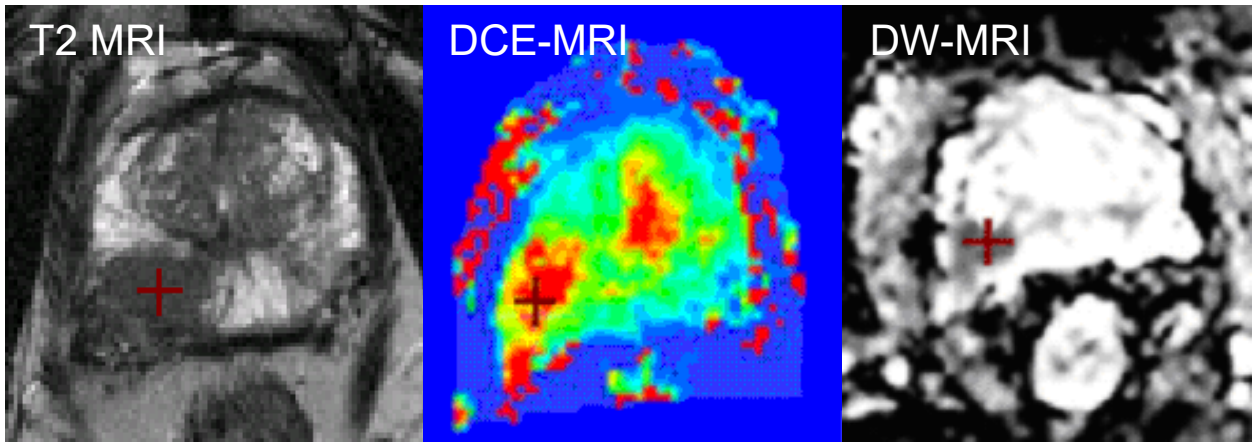
Using multi-parametric imaging to differentiate dose inside the target volume

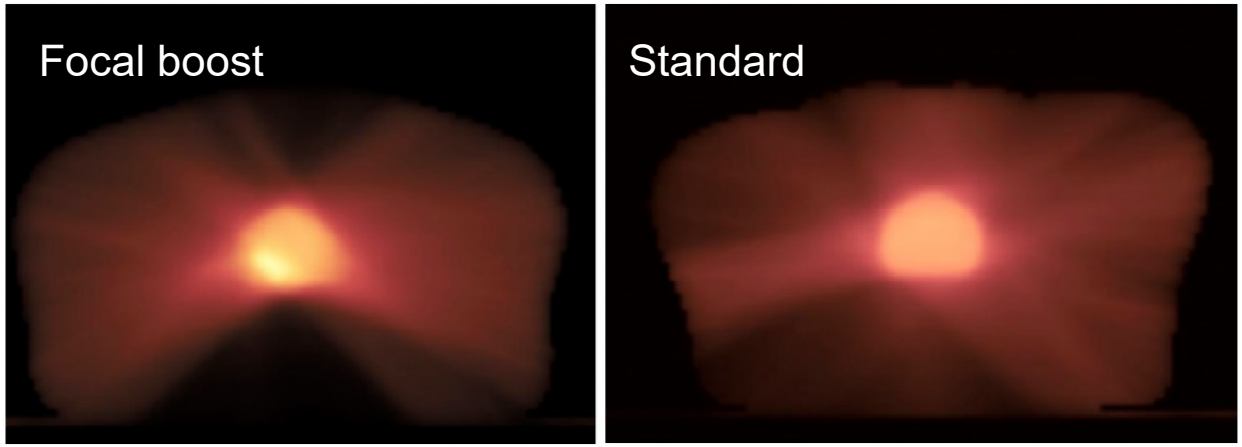
Example: prostate cancer

Standard: homogeneous dose to entire prostate

New: escalate dose at location of highest tumor burden

What about uncertainties?

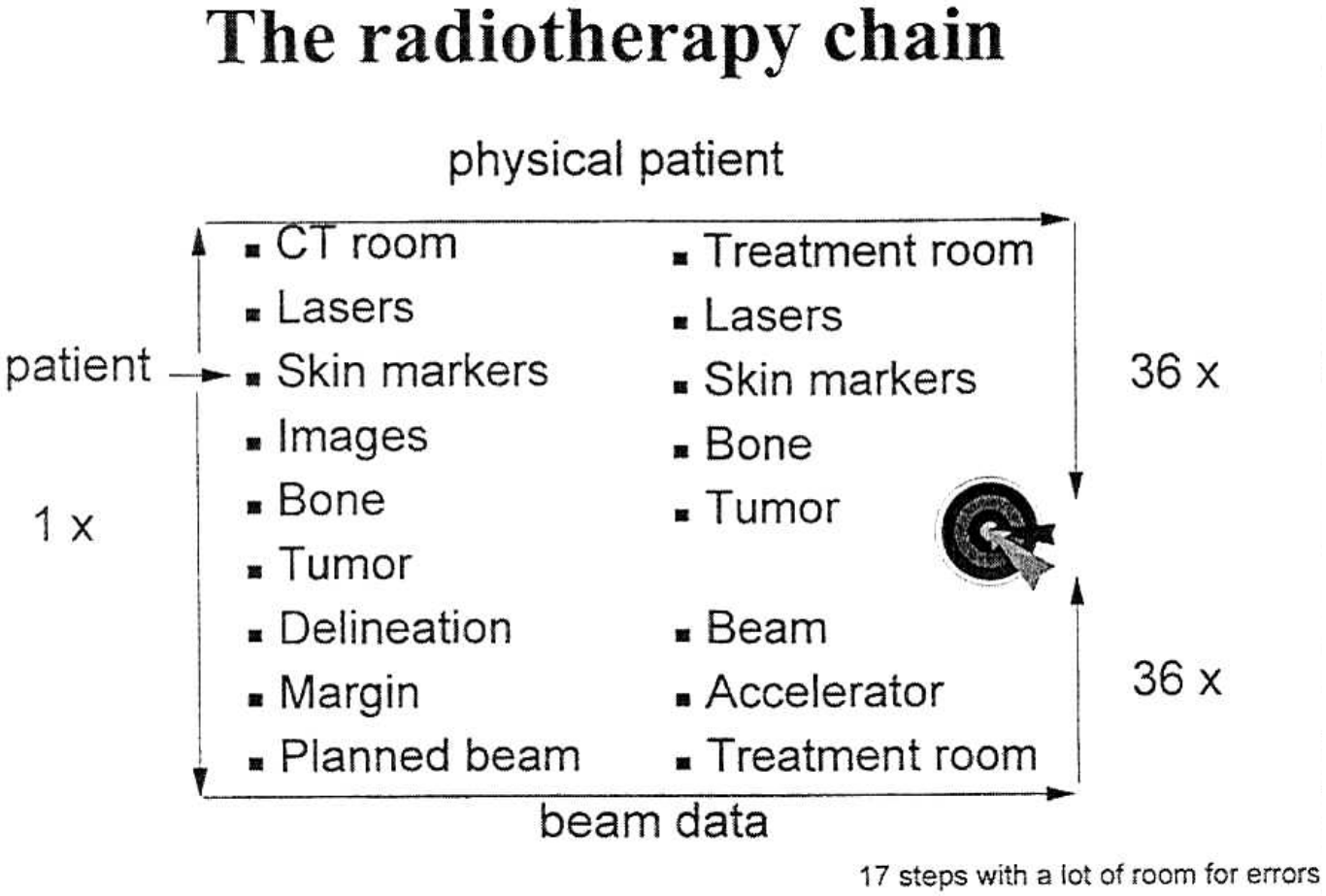




Uncertainties to consider

PTV margins are intended to guarantee that x% of patients receive a minimum dose of ≥ y% of the prescribed dose

- Usually 90% of patients, at least 95% of the dose



Courtesy Marcel van Herk

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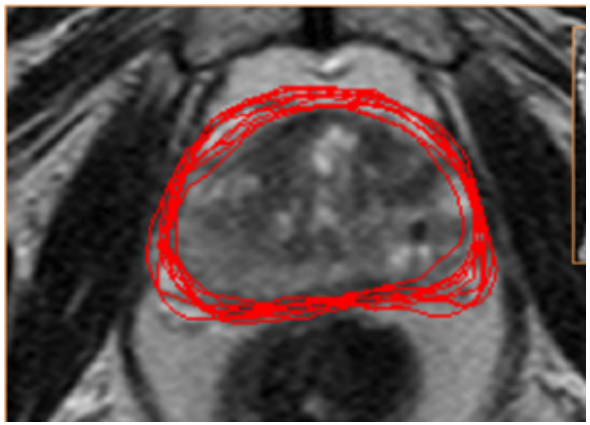
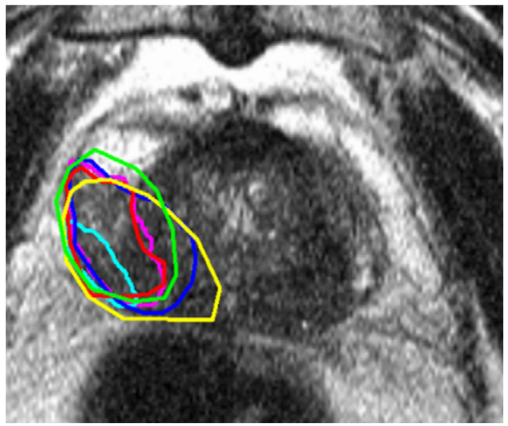
Uncertainties to consider: target definition

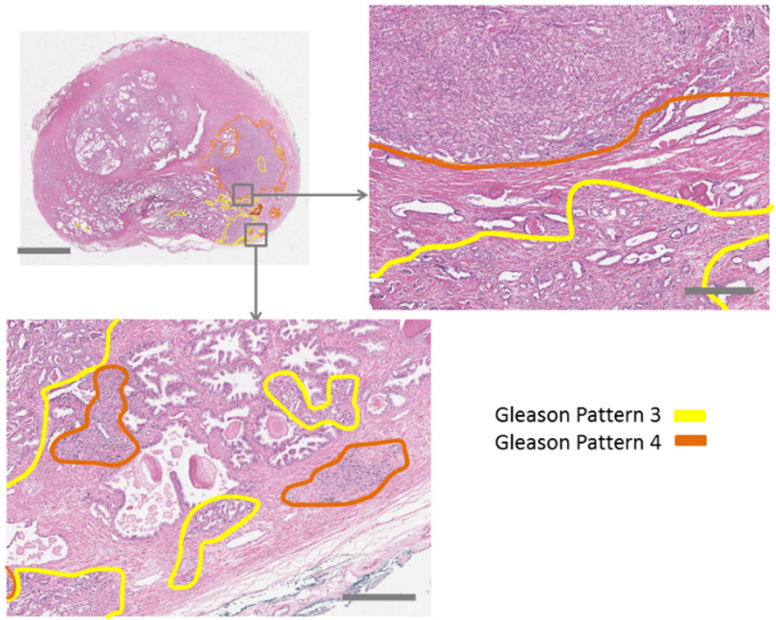
Delineation uncertainties

- Prostate
- Tumor



Nyholm et al. 2013; Radiat Oncol.





Steenbergen et al. 2015; Radiat Oncol.

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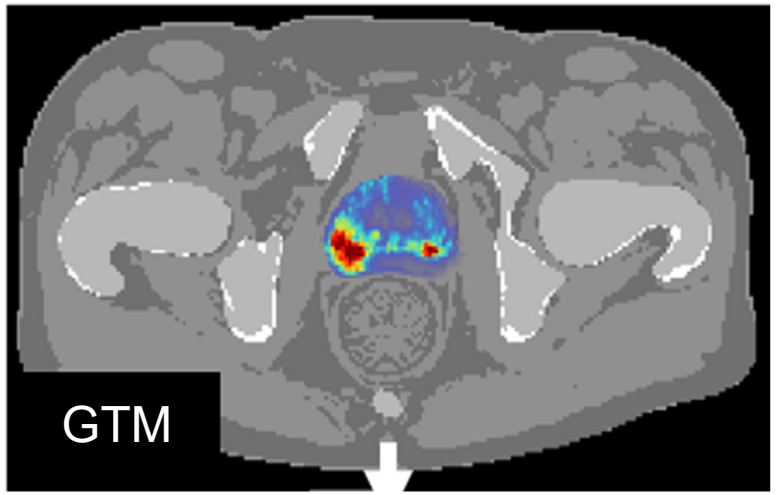
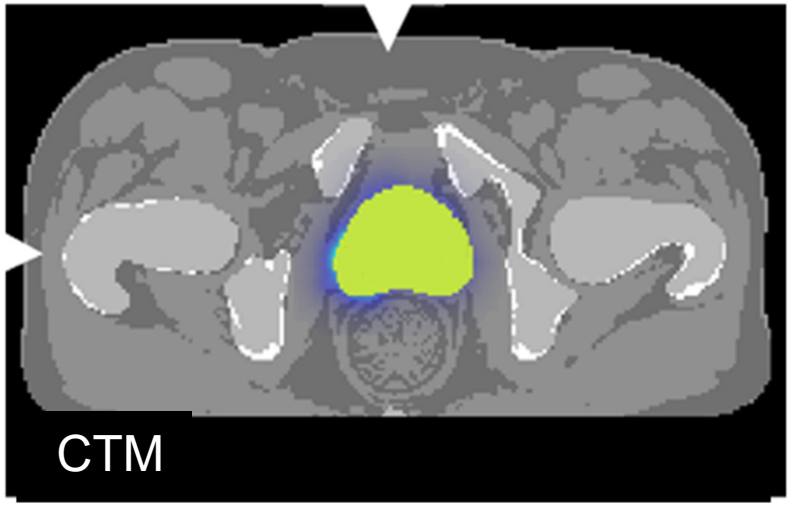
Towards a probabilistic definition of target volumes



Express uncertainty in the target definition by probabilities

‘Gross Tumor Volume’ becomes ‘Gross Tumor Map’

Towards a probabilistic definition of target volumes



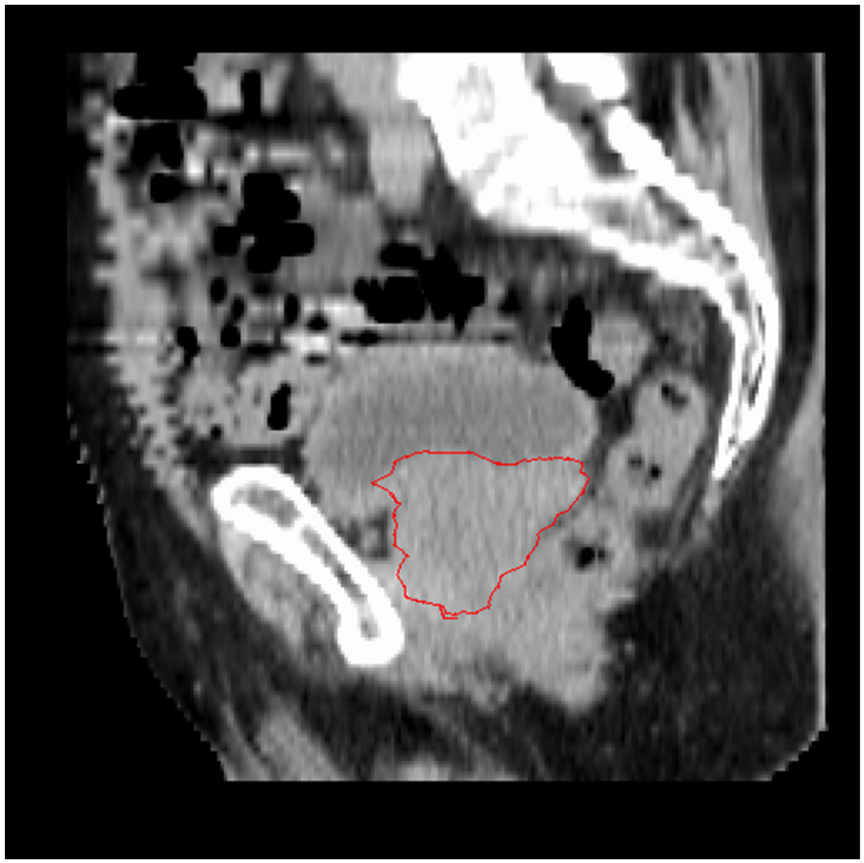
Express uncertainty in the target definition by probabilities
Include likelihood of extra-capsular disease

‘Clinical Tumor Volume’ becomes ‘Clinical Tumor Map’

Uncertainties to consider: positioning uncertainties

Organ motion

- Inter-fraction motion



Courtesy Marcel van Herk

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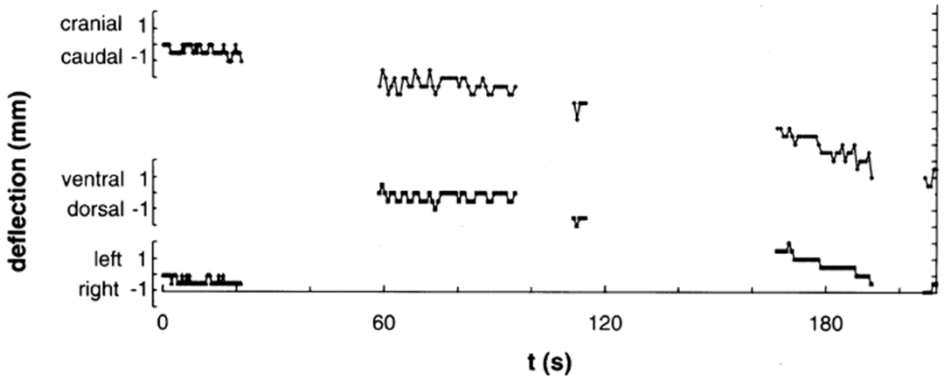
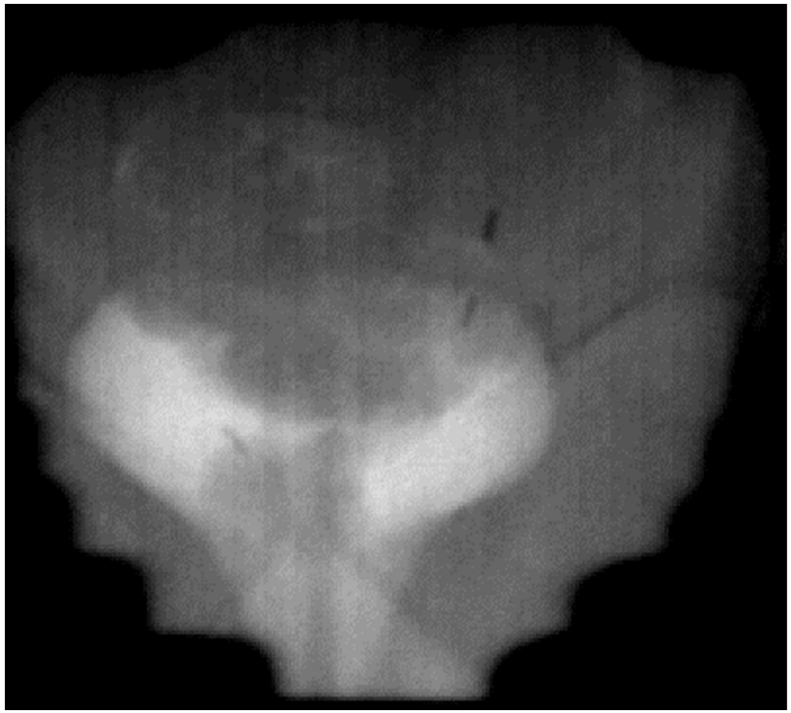
Uncertainties to consider: positioning uncertainties

Organ motion

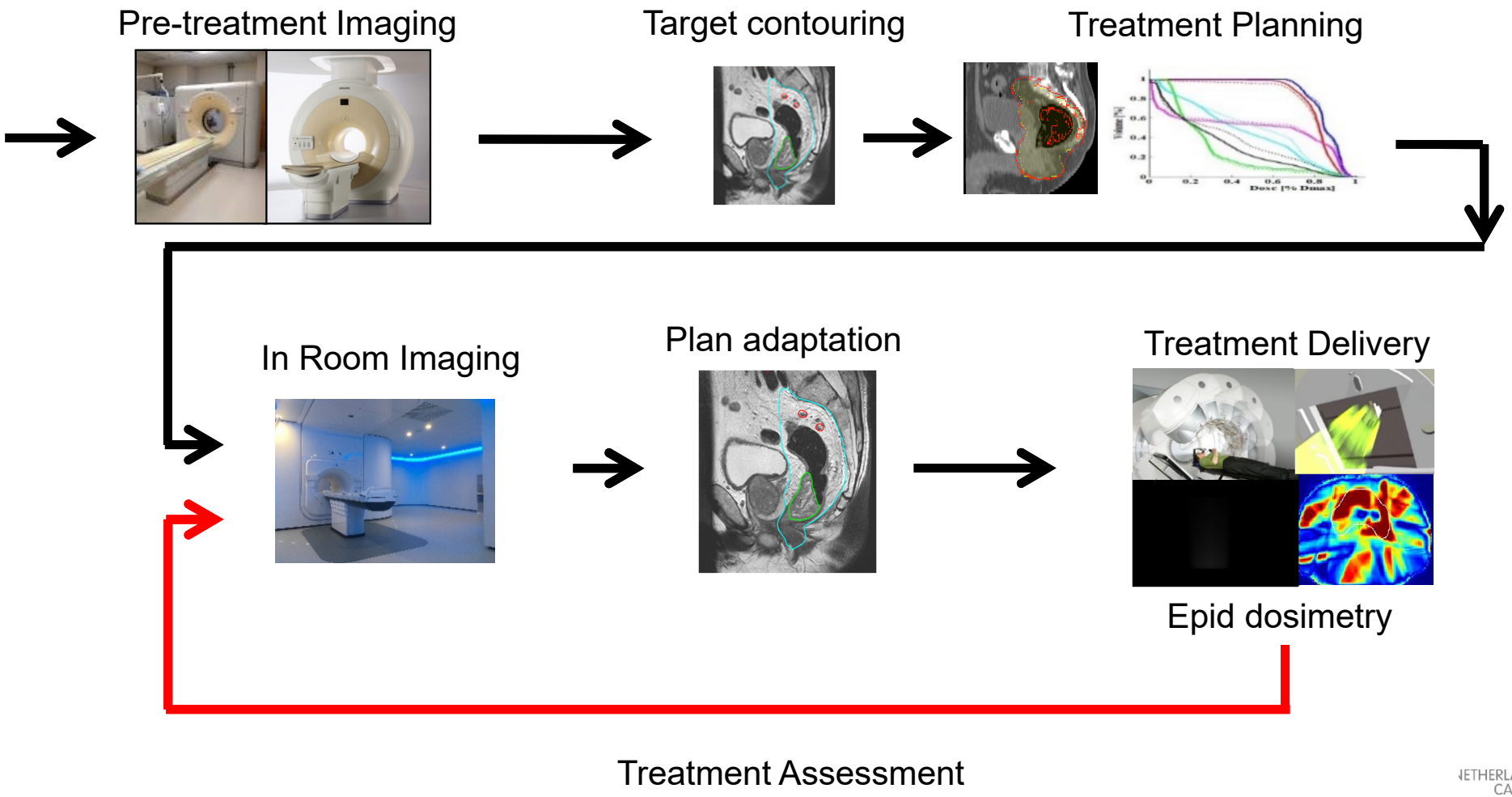
- Inter-fraction motion
- Intra-fraction motion





Nederveen et al. Int J Radiat Oncol Biol Phys. 2002 May 1;53(1):206-14

Adapt each fraction to the changing shape of the target



MRI-guided radiotherapy

ATP: “Adapt to Position”

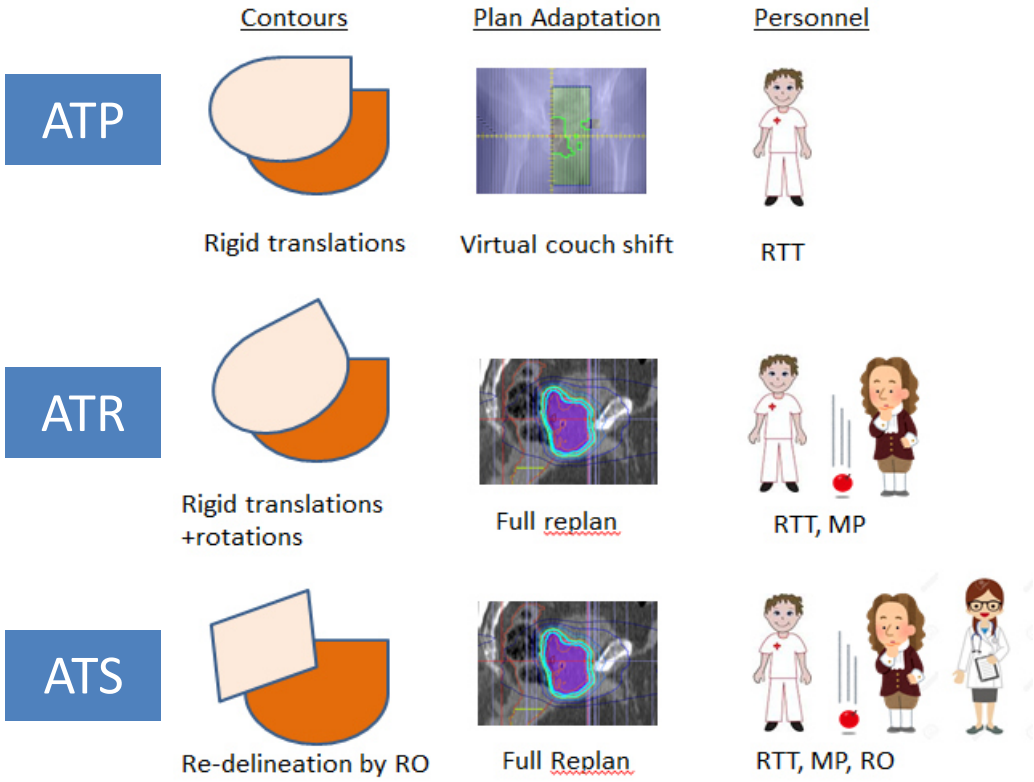
(virtual) couch shift

ATR: “Adapt to Rotation”

Shift and rotate targets rigidly and replan; no re-contouring

ATS: “Adapt to Shape”

Full adaptation



ICRU report 97: MRI-Guided Radiation Therapy Using MRI-Linear Accelerators

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Uncertainties in on-line adaptive radiotherapy

	ATP	ATR	
Simulation/treatment planning			
Match uncertainty planning CT and planning MRI	S	S	
Contouring uncertainty	S	S	
On-line treatment			
Match uncertainty planning CT and adaptation MRI	R	R	
Contouring uncertainty	-	-	
Geometrical uncertainties of the linac	S/R	S/R	
Intra-fraction motion	R	R	

Uncertainties in on-line adaptive radiotherapy

	ATP	ATR	ATS
Simulation/treatment planning			
Match uncertainty planning CT and planning MRI	S	S	-
Contouring uncertainty	S	S	-
On-line treatment			
Match uncertainty planning CT and adaptation MRI	R	R	-
Contouring uncertainty	-	-	R
Geometrical uncertainties of the linac	S/R	S/R	S/R
Intra-fraction motion	R	R	R

Systematic errors may become random in an on-line adaptive workflow

Assumptions in the ‘van Herk recipe’ $m_{PTV} = 2.5 \Sigma + 0.7 \sigma$

The dose gradient is described with σ_p =3.2 mm

90% of patients receives a minimum dose of ≥ 95% of the prescribed dose

Van Herk, Remeijer; Int. J. Radiat. Oncol. Biol. Phys., Vol. 47, No. 4, pp. 1121–1135, 2000

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10% of patients must not receive the prescribed dose

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Assumptions in the 'van Herk recipe' $m_{PTV} = 2.5 \Sigma + 0.7 \sigma$

The dose gradient is described with σ_p =3.2 mm

90% of patients receives a minimum dose of ≥ 95% of the prescribed dose

10% of patients must not receive the prescribed dose
(but not a whole lot less)

Van Herk, Remeijer; Int. J. Radiat. Oncol. Biol. Phys., Vol. 47, No. 4, pp. 1121–1135, 2000

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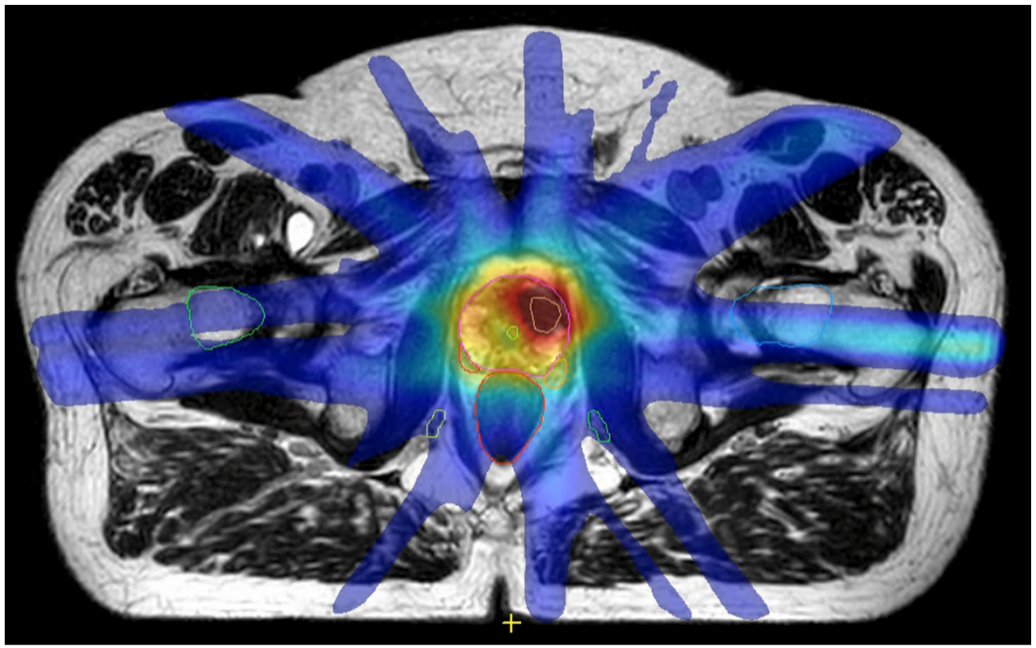
Destination

Low-intermediate risk prostate cancer

5 fractions

GTV: isotoxic boost up to 45 Gy

CTV (prostate): 30 Gy



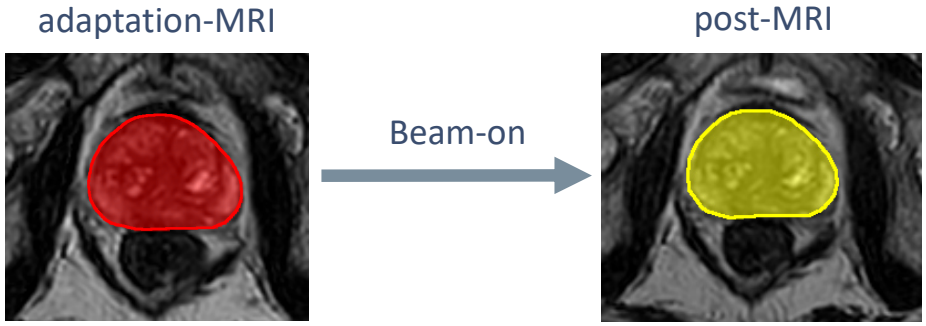
Planning study

23 patients with intermediate risk prostate cancer treated on Elekta Unity 1.5T

T2w MRIs available for adaptation and post-treatment in 5 fractions

GTV: 45 Gy, CTV 30 Gy

PTV = 0 mm



Time interval between adaptation- and post-MRI mean 18 min [14-27]

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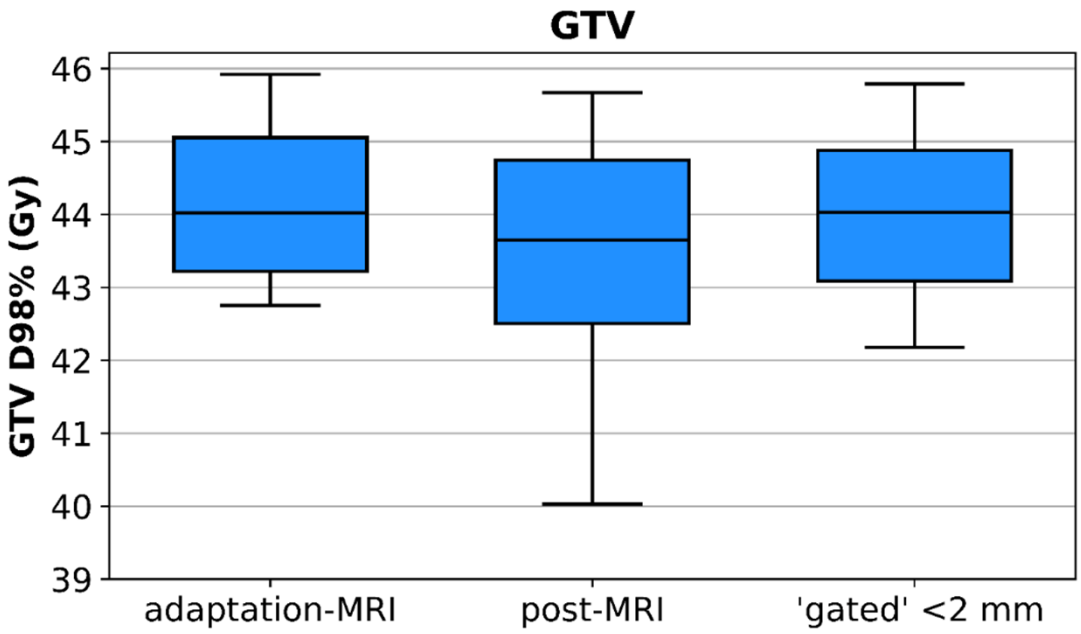
Dose coverage of the GTV

D98% > 40 Gy in 90% of fractions

When correcting intra-fraction motion > 2 mm: D98% > 42 Gy in 90% of fractions

Analysis per fraction, renormalized to 5 fractions



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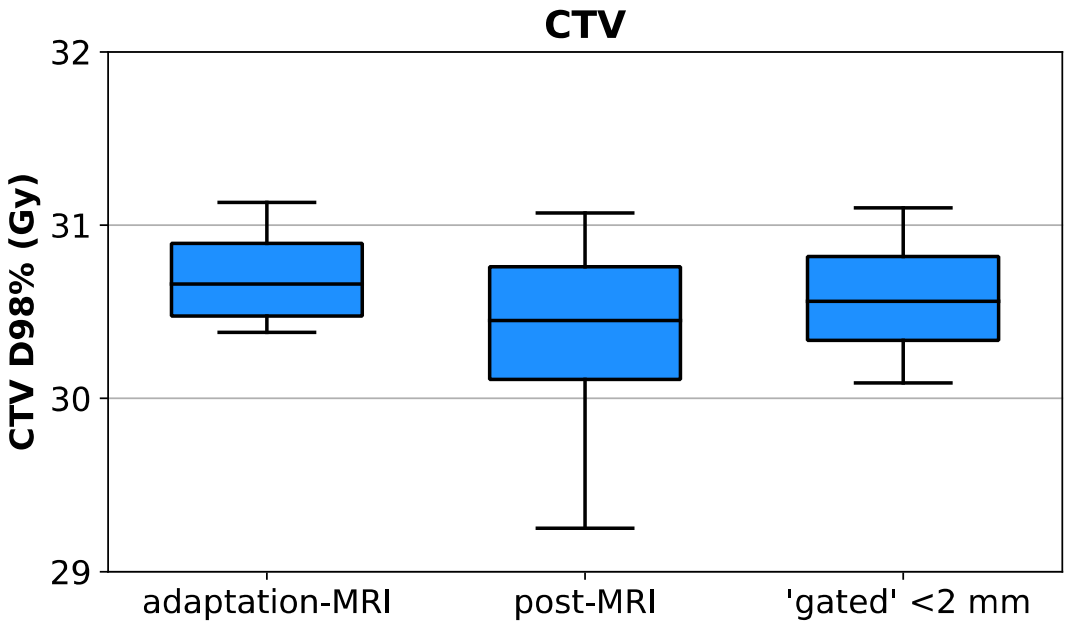
Dose coverage of the CTV

D98% > 29 Gy in 90% of fractions

When correcting intra-fraction motion > 2 mm: D98% > 30 Gy in 90% of fractions

Analysis per fraction, renormalized to 5 fractions



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Assumptions in the ‘van Herk recipe’ $m_{PTV} = 2.5 \Sigma + 0.7 \sigma$

The dose gradient is described with σ_p =3.2 mm

90% of patients receives minimally the prescribed dose

Tumor cells are homogeneously distributed in the target volume

Van Herk, Remeijer; Int. J. Radiat. Oncol. Biol. Phys., Vol. 47, No. 4, pp. 1121–1135, 2000

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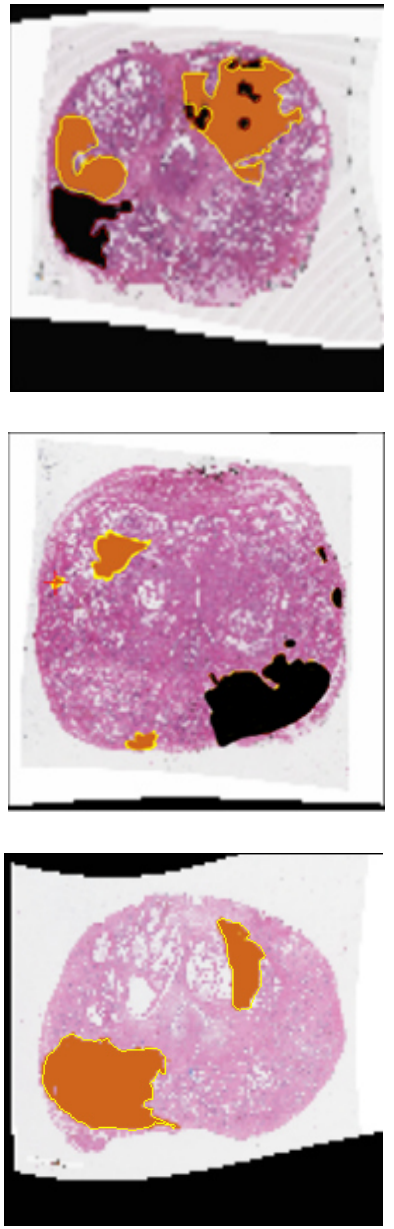
Can we estimate the tumor load in the CTV?

61 prostatectomy specimen

84% of patients had multifocal disease (median 3 foci)

32% of foci smaller than 5 mm diameter

Contribution of small foci to total tumor load 2%



Hollmann et al. Radiother Oncol. 2015 Apr;115(1):96-100

Implications for PTV margins

For CTV the inhomogeneous distribution of tumor cells is not considered in the classical margin recipes

There is a high probability that the underdosed volume contains no cancer at all

The dose doesn’t fall to zero

Modern dose distributions: what we shouldn’t forget

To express uncertainty, a probabilistic target definition is desirable

With on-line adaptive radiotherapy, positioning errors are substantially reduced

With ultra-hypofractionation, (almost) all errors become systematic

The tumor cells are not homogeneously distributed inside the CTV. This has profound implications for the required PTV margin

Acknowledgements

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